

# Supplementary Material: Unsupervised Domain Adaptation for Tubular Structure Segmentation Across Different Anatomical Sources

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## 1 Data Preprocessing

We used four datasets in this paper to validate the effectiveness of our approach, ISBI [2], VNC [8], DRIVE [14], and CHASE [6]. Electron microscope images (ISBI and VNC) are grayscale images and fundus images (DRIVE and CHASE) are RGB three-channel color images. Therefore we grayscaled the fundus images. Since the regions of interest of electron microscope images and fundus images are different, the region of interest of electron microscope images is the set of all pixels, and the region of interest of fundus images is the set of pixels inside the eyeball. To prevent incomplete global information and reduce discrepancies caused by patching, we rescaled all images to  $512 \times 512$  using cubic interpolation. Simultaneously, labels were resized to the corresponding  $512 \times 512$  size using nearest neighbor interpolation. Our enhanced images are obtained by summing the feature maps obtained by Jerman [10] and Frangi [5] after black and white conversion with the original image.

### 1.1 Comparison Experiments

We validate the effectiveness of our approach with a comprehensive comparison of nine unsupervised domain adaptation methods on four datasets. These nine methods are DANN [2], UMDA-SNA [10], DCDA [10], SAM-UDA [8], ADANet [14], FFO [14], SFUDA [8], MIC [8], and LA-UDA [8]. Figure 1 demonstrates the complete comparison results. Table 1 quantifies the metrics differences between the different UDA methods, showing that the segmentation results of our method are more accurate. Our method is able to obtain more continuous and more complete segmentation results in fundus images, which is more obvious at the ends of blood vessels. Our approach yields segmentation outcomes with reduced noise in electron microscopy images. Furthermore, it achieves more precise segmentation

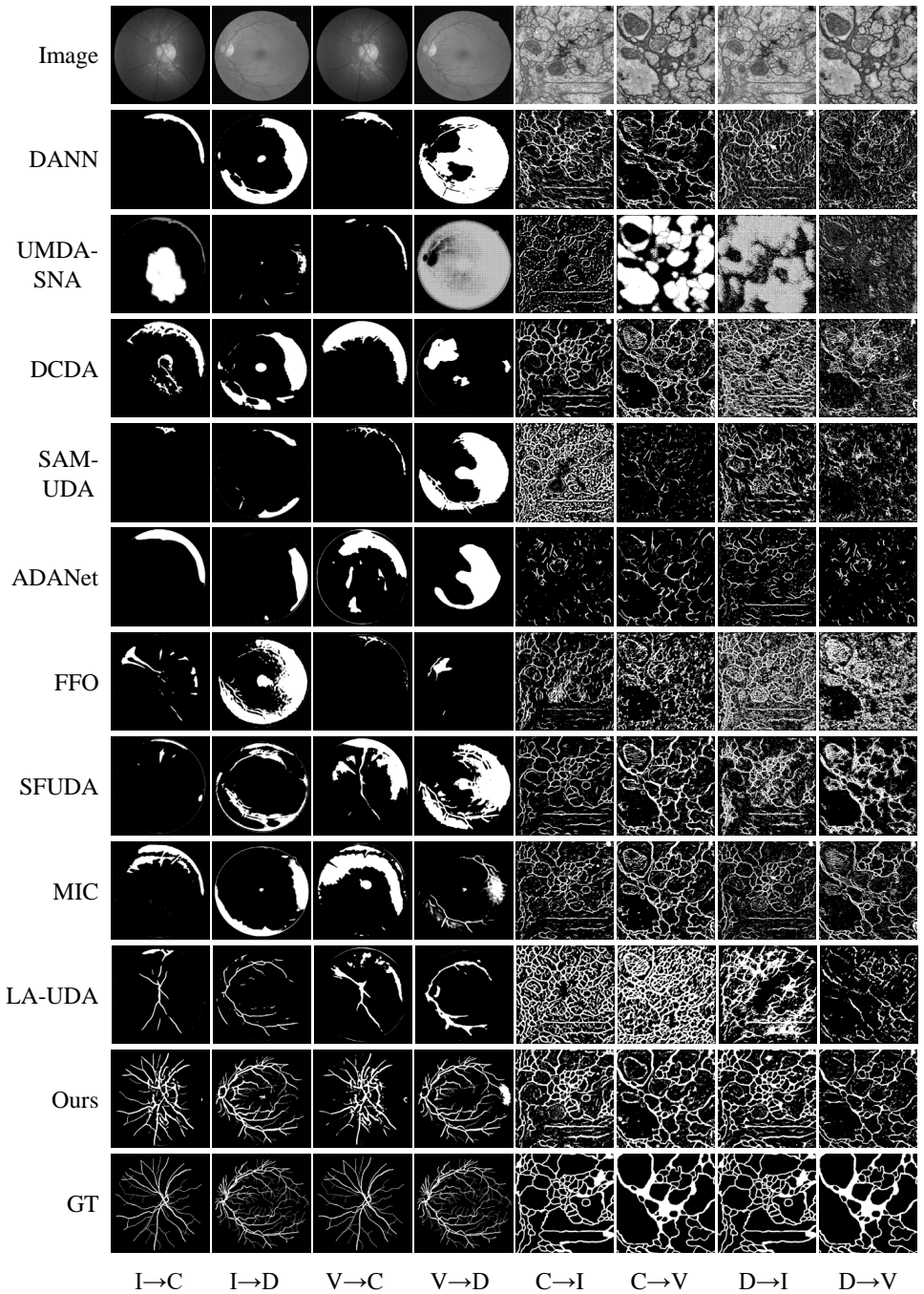


Figure 1: Visualization examples of comparative experiments. I: ISBI, V: VNC, C: CHASE, D: DRIVE.

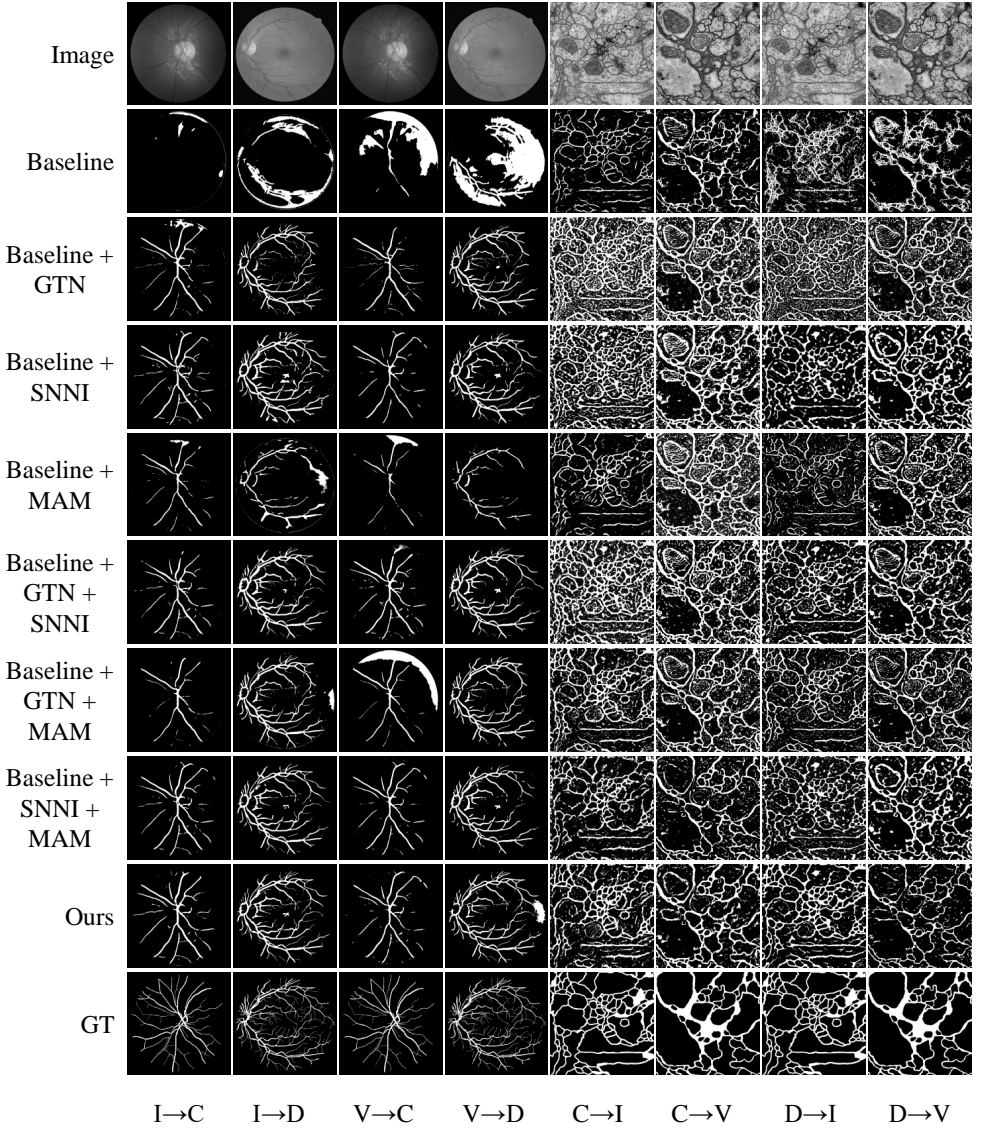


Figure 2: Visualization examples of ablation studies. I: ISBI, V: VNC, C: CHASE, D: DRIVE.

results for the thicker regions of the tubular structure. The results of the comparison experiments demonstrate that UDA methods proposed for a single anatomical source do not work well in a multi-anatomical source setting. We believe that this is due to the variability in the data characteristics of the tubular structures of different anatomical sources and the great variability in the background noise of different anatomical sources. In addition, the fact that these methods do not provide explicit feature constraints for the segmentation targets is also a reason for their failure.

Table 1: Comparison experiments. I: ISBI, V: VNC, C: CHASE, D: DRIVE.

Method	I→C	I→D	V→C	V→D	C→I	C→V	D→I	D→V
U-Net(No adaptation) [14]	7.79%	2.88%	16.56%	22.84%	36.13%	20.13%	36.79%	27.76%
U-Net(Supervised) [14]	80.59%	80.87%	80.59%	80.87%	78.73%	88.30%	78.73%	88.30%
DANN [15]	12.34%	13.75%	13.43%	19.27%	57.88%	62.81%	47.88%	44.84%
UMDA-SNA [16]	15.87%	10.85%	13.75%	21.35%	42.36%	32.24%	37.70%	19.57%
DCDA [17]	15.92%	14.17%	16.33%	20.16%	61.23%	63.06%	46.59%	45.28%
SAM-UDA [18]	14.10%	10.78%	13.92%	16.89%	43.43%	39.95%	40.35%	22.83%
ADANet [19]	11.43%	9.69%	14.31%	12.49%	65.40%	36.48%	41.69%	23.56%
FFO [20]	19.73%	18.13%	14.80%	20.04%	48.57%	36.67%	46.90%	35.33%
SFUDA [21]	13.79%	26.40%	14.80%	26.43%	54.44%	64.75%	54.15%	59.51%
MIC [22]	15.42%	10.86%	14.85%	15.13%	61.85%	68.74%	59.14%	64.57%
LA-UDA [23]	36.76%	39.70%	24.67%	26.34%	56.19%	44.15%	45.29%	47.80%
Ours	<b>60.46%</b>	<b>67.11%</b>	<b>53.93%</b>	<b>61.68%</b>	<b>67.52%</b>	<b>70.84%</b>	<b>68.05%</b>	<b>69.94%</b>

Table 2: Ablation studies. I: ISBI, V: VNC, C: CHASE, D: DRIVE.

Method	I-C	I-D	V-C	V-D	C-I	C-V	D-I	D-V
Baseline	13.79%	26.40%	14.80%	26.43%	54.44%	64.75%	54.15%	59.51%
Baseline+GTN	51.92%	60.62%	36.47%	59.00%	53.26%	57.48%	56.42%	58.82%
Baseline+SNNI	56.60%	63.23%	50.79%	60.96%	54.79%	63.06%	62.36%	64.99%
Baseline+MAM	55.06%	34.30%	43.36%	36.24%	65.89%	57.01%	60.02%	62.03%
Baseline+GTN+SNNI	55.98%	64.38%	52.10%	61.29%	55.42%	60.95%	61.22%	65.73%
Baseline+GTN+MAM	34.28%	57.25%	27.67%	57.48%	64.29%	63.60%	64.47%	62.53%
Baseline+SNNI+MAM	59.35%	64.48%	53.32%	59.24%	64.54%	66.66%	63.04%	65.92%
Ours	<b>60.46%</b>	<b>67.11%</b>	<b>53.93%</b>	<b>61.68%</b>	<b>67.52%</b>	<b>70.84%</b>	<b>68.05%</b>	<b>69.94%</b>

## 1.2 Ablation Studies

We verify the effectiveness of the three proposed modules in the framework through ablation studies. We use the segmentation network in [14] as a baseline and attach the proposed modules to the framework separately. The ablation results show that all three of our proposed modules improve the segmentation accuracy. Figure 2 shows visualization results of ablation studies. Table 2 lists the quantitative results of the ablation studies. Through ablation studies, we also found that in some cases, the performance of using GTN and MAM is not as good as using either of the two modules alone. We believe that the use of GTN + MAM drives the model to refine the segmentation of the source domain without enhancing the segmentation network, thus decreasing the segmentation performance of the target domain. The effectiveness of the two combinations, GTN + SNNI and SNNI + MAM, proves our theory.

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