Human Activity Tracking from Moving Camera Stereo Data

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Abstract

We present a method for tracking human activity using observations from a moving narrow-baseline stereo camera. Range data are computed from the disparity between stereo image pairs. We propose a novel technique for calculating weighting scores from range data given body configuration hypotheses. We use a modified Annealed Particle Filter to recover the optimal tracking candidate from a low dimensional latent space computed from motion capture data and constrained by an activity model. We evaluate the method on synthetic data and on a walking sequence recorded using a moving hand-held stereo camera.

1 Introduction

Annealed Particle Filtering (APF) has been shown to recover 3D human motion consistently using observations from 3 or more cameras [5, 7]. Silhouettes are used in the calculation of agreement between image evidence and body configuration hypotheses, or weighting function. Background subtraction is difficult to achieve without a well controlled experimental environment where backgrounds and sensor position are stationary. Using fewer than 3 cameras, where standard APF tracking fails rapidly [5], statistical models of human activity have been successfully used to constrain the search problem [14, 15, 17]. Offline estimation of joint locations using a 2D image-based tracker [16, 17] or assumptions about known backgrounds for silhouette extraction [11, 15] are common and the robustness to changing illumination, backgrounds, subject appearance and sensor position is limited.

A narrow-baseline stereo camera provides synchronised image pairs of a scene from 2 close-mounted parallel cameras. Processed as part of a multi-camera wide-baseline tracking scheme [7] the observations are so similar that their combination offers negligible benefit over monocular tracking performance. However, by calculation of the disparity between the paired images, range information for objects in the scene can be estimated at video frame rates [10]. In general, stereo range data provides a noisy image cue. Range accuracy is affected by errors in camera alignment and calibration while range resolution – the minimum discernable change in distance – increases as the square of the range. The issue of accuracy has led some approaches to human motion tracking to exclude stereo

range data from their calculation of hypothesis weightings [4]. We propose an activity-supervised APF method, summarised in Figure 1, to achieve robust tracking from range data. We will argue that when incorporated with an activity model, the stereo range data alone is sufficiently rich for tracking using a particle filtering approach.

Motivated by the use of chamfer images to calculate weightings from edge features in the APF algorithm [7], we introduce a chamfer volume method to compute weightings from surface features. We discretise 2.5D surface range data before smoothing it with a 3D Gaussian kernel (Section 3.3). The result is a chamfer volume where each voxel's magnitude is proportional to its distance to a surface. We use a modified APF scheme to search for the optimum body configuration at each frame, based on comparisons between the visible surfaces of a simple body model and the chamfer volume (Section 3.2). Body configuration hypotheses are drawn from a low dimensional activity subspace recovered from motion capture (MoCap) data by Principal Components Analysis (PCA). The activity space is constrained by training a hidden Markov model (Sections 3.1) which provides a model of activity dynamics and prohibits the sampling of illegal pose regions. The approach retains the reduced computational expense of PCA over nonlinear techniques (Section 2) and we hope to extend it to consider multiple activity models in multiple activity spaces in future work (Section 5). We test the proposed tracking approach using synthetic data and a sequence featuring a walking subject recorded by a moving hand-held stereo camera (Section 4).

2 Related Work

In the general case – tracking human motion where sensor evidence is weak – there have been many contributions based on the use of prior models of human behaviour. A common application is human motion tracking from monocular sequences where available image evidence is particularly ambiguous. Linear dimensionality reduction techniques such as PCA have been applied to activity training data to impose feature space constraints in the search for an optimum tracking candidate [14, 18]. Invertible nonlinear dimensionality reduction techniques such as Locally Linear Coordination (LLC) and the Gaussian Process Latent Variable Model (GPLVM) have been shown to recover rich low dimensional pose spaces from which a mapping back to the original feature space is available [11, 17]. None of PCA, LLC or GPLVM are dynamical models, and further steps must be taken to model temporal relationships in the data. For example, Hou et al. capture dynamics at different temporal scales by learning a Variable Length Markov Model from clusters in the latent space [8]. The Gaussian Process Dynamical Model [19] represents a combined approach, recovering a nonlinear low dimensional latent space and model of temporal dynamics within a single learning algorithm [16, 13].

Several approaches have incorporated stereo range data into the human motion tracking problem. The Iterative Closest Point algorithm (ICP) was used by Demirdjian to find the transformation between a set of 3D points on a body model and a set of range data coordinates [6]. Articulated body model constraints were modelled by the projection of the unconstrained body model transformation onto a linear articulated motion space. Azad et al. [3] considered other image cues in addition to range data, segmenting the hands and head of the subject by colour and locating their corresponding 3D positions in range evidence. The result was used to constrain the feature space explored by a particle filter

which incorporated edge and region information into its weighting calculation. Both approaches used relatively simple body models composed of rigid primitives for limbs and were shown to track sequences of upper body movement featuring some self occlusion.

Jojic et al. [9] used a body model described by an articulated set of 3D Gaussian 'blobs'. Tracking was performed using Expectation-Maximisation and articulated constraints enforced by an Extended Kalman Filter. Real time tracking of head and arm movements was demonstrated on a sequence featuring some self-occlusion. Plänkers and Fua employed a sophisticated deformable body model to track using range and silhouette data estimated from a trinocular video sequence [12]. A set of Gaussian density distributions, or 'metaballs' were used to form an Articulated Soft Object Model (ASOM). The form of the ASOM allows for the definition of a distance function to range data that is differentiable and so the weighting function may be maximised using deterministic optimisation methods. The parameters of the ASOM were estimated in a frame-to-frame tracking stage by minimisation of the objective function given range data, before being refined by a global optimisation over all frames. Remarkable upper body tracking results were demonstrated on sequences of a bare-skinned subject performing abrupt arm waving and featuring self occlusion. ASOMs were later used for comparison with stereo range data featuring walking and running [18]. Full body tracking was achieved by minimising the objective function with respect to the first 5 coefficients of a pre-computed activity space recovered from MoCap training data using PCA.

3 Formulation

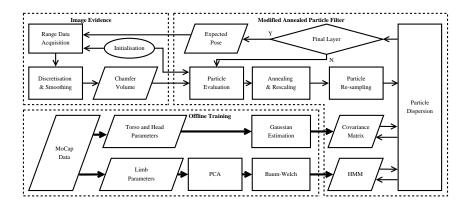


Figure 1: Activity-supervised APF for range image tracking.

3.1 Modelling Activity

Our body model comprises a kinematic tree with 10 truncated cones described by a 31-parameters body vector representing the torso position and orientation and the pose via relative joint angles between limbs. These body parameters can be recovered from accurate MoCap and we use m=1,...,M walking body vectors [5] to construct our activity

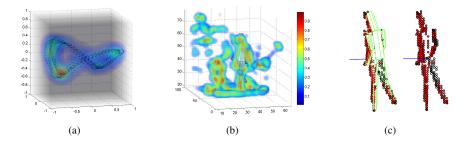


Figure 2: Activity model, chamfer volume and body model. (a) Latent walking data and resulting HMM observation densities; (b) Chamfer volume and body model hypothesis; (c) Rotated body model showing the extracted sample coordinates and effects of intra-and inter-cone occlusion.

model. We downsample to 30fps and remove the 9 parameters of each body vector describing the torso and head, ϵ'_m , as we do not want a subject's route or line of sight to form part of the generic activity class. PCA is performed on the sequence of remaining 22D limb parameter vectors $E = \{\epsilon_1, ..., \epsilon_M\}$. By retaining the eigenvectors corresponding to the 4 largest eigenvalues $\Phi = (\phi_1|...|\phi_4)$, we preserve 93% of the variance. The data can then be approximated by the sequence of weighting vectors $F = \{\mathbf{f}_1, ..., \mathbf{f}_M\}$ using $\epsilon_m \approx \bar{\epsilon} + \Phi \mathbf{f}_m$. Figure 2(a) shows the body configuration trajectory projected onto the 3 highest variance eigenvectors. The full feature vector is 13D, comprising the 9 torso and head parameters and the approximation of the remaining limb parameters given by the 4D weighting vector, $\mathbf{x}_m = (\epsilon'_m, \mathbf{f}_m)$.

A hidden Markov model (HMM) can be used to model a time series of observations such as $F = \{\mathbf{f}_1, ..., \mathbf{f}_M\}$ where the sequence of observations is the result of a doubly stochastic process. An HMM λ is specified by the parameters $S, A_{ij}, A_i, p_i(\mathbf{f})$, where $S = \{s_1, ..., s_N\}$ is the set of states; the $N \times N$ matrix A_{ij} gives the probability of a transition from state i to state j; A_i gives the probability of a sequence starting in state i and $p_i(\mathbf{f})$ is the probability of observing feature vector \mathbf{f} while in state i. We model each observation density by a single multivariate Gaussian $p_i(\mathbf{f}) = \mathcal{N}(\mathbf{f}|\boldsymbol{\mu}_i, \boldsymbol{\Sigma}_i)$ with mean $\boldsymbol{\mu}_i$ and covariance $\boldsymbol{\Sigma}_i$. HMM training is performed using the Baum-Welch algorithm with initial estimates for $\boldsymbol{\mu}_i$ and $\boldsymbol{\Sigma}_i$ found by k-means clustering, A_{ij} randomised and A_i held constant as a flat distribution. Figure 2(a) shows a visualisation of the observation densities recovered by training a 15 state HMM on walking data F.

3.2 Temporal Dynamics for APF

If human motion is recorded using a stereo camera then by assuming that the set of observations $\mathbf{Z}_m = (\mathbf{z}_1,...,\mathbf{z}_m)$ are independent and that the evolution of the body's configuration is a first order Markov process, the state density may propagated using

$$p(\mathbf{x}_m|\mathbf{Z}_m) \propto p(\mathbf{z}_m|\mathbf{x}_m) \int_{\mathbf{x}_{m-1}} p(\mathbf{x}_m|\mathbf{x}_{m-1}) p(\mathbf{x}_{m-1}|\mathbf{Z}_{m-1}).$$
 (1)

SIR [2] allows for the representation of a multimodal posterior, $p(\mathbf{x}_m|\mathbf{Z}_m)$, with a set of normalised, weighted particles, $\{(\mathbf{x}_m^{(1)}, \pi_m^{(1)}), ..., (\mathbf{x}_m^{(B)}, \pi_m^{(B)})\}$. Dispersion by a model of

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Initialisation: \{(\mathbf{x}_1^{(b)}, 1/B)\}_{b=1}^B. for m=1 to M do for r=R downto 1 do 1. Calculate weights \pi_m^{(b)} = w_m^r(\mathbf{z}_m, \mathbf{x}_m^{(b)}).

2. Resample B particles with likelihood \propto \pi_m^{(b)} and with replacement.

3. Find most likely parent state of limb parameters: \arg\max_i(p_i(\mathbf{f}_m^{(b)})).

4. Rescale dispersion parameters \mathbf{P}_r, \mathbf{\Sigma}_i^r and \rho_T^r by \alpha^r.

5. Make K_i^r = \left\lceil \frac{\ln(1-\rho_T^r)}{\ln(A_{ii})} \right\rceil state transitions via A_{ij} and emit an observable: if j \neq i then \mathbf{f}_m^{(b)} = p_j(\mathbf{f}) = \mathcal{N}(\mathbf{f}|\boldsymbol{\mu}_j, \mathbf{\Sigma}_j^r). else \mathbf{f}_m^{(b)} = p_i'(\mathbf{f}) = \mathcal{N}(\mathbf{f}|\boldsymbol{\mu} = \mathbf{f}_m^{(b)}, \mathbf{\Sigma}_i^r). end if 6. Disperse head and torso parameters \boldsymbol{\epsilon}'_m = \mathcal{N}(\boldsymbol{\epsilon}'|\boldsymbol{\epsilon}'_m, \mathbf{P}_r).

7. Concatenate to give new particle location \mathbf{x}_m^{(b)} = (\boldsymbol{\epsilon}'_m, \mathbf{f}_m^{(b)}). end for Calculate expected configuration for visualisation \mathcal{E}(\mathbf{x}_m) = \sum_{b=1}^B \pi_m^{(b)} \mathbf{x}_m^{(b)}. end for
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Figure 3: Pseudocode for particle dispersion.

temporal dynamics (usually drift-and-spread), evaluation by a weighting function $w(\mathbf{z}_m, \mathbf{x}_m^{(b)}) \approx p(\mathbf{z}_m | \mathbf{x}_m^{(b)})$ and resampling with probability proportional to weighting score $\pi_m^{(b)}$, propagates the posterior approximation over time.

APF [7] has been shown to give increased tracking accuracy [5] by cooling the weighting distribution and then gradually introducing sharp peaks over r = R, R - 1, ..., 1 separate resampling layers at each time step m:

$$w_m^r(\mathbf{z}_m, \mathbf{x}_m) = w(\mathbf{z}_m, \mathbf{x}_m)^{\beta_m^r}, \quad \beta_m^1 > \beta_m^2 > \dots > \beta_m^R.$$
 (2)

The value of β_m^r is chosen to control the particle survival rate α^r , the proportion of particles that will be resampled. The aim of APF is to recover the hypothesis that maximises the weighting function, generally leading to a concentration of particles into a particular mode of the distribution. The posterior distribution is not fully represented, leading to a reduction in weighting function evaluations at the expense of a departure from the formal Bayesian framework.

Rather than using drift-and-spread dynamics [4] or adding noise [15] we appeal to the pre-trained activity HMM to disperse the weighting vector parameters, finding $\mathbf{f}_m|\mathbf{f}_{m-1}$ and therefore the limb parameters $\boldsymbol{\epsilon}_m$. The annealing process can cause APF to recover the wrong interpretation when faced with multiple maxima of approximately equal magnitude in the posterior [5]. Similarly, high densities of samples in a relatively flat posterior may cause the particle set to 'stall'. Where there are considerably fewer HMM states than training data per activity cycle, each state has a high probability of undergoing a self-transition. This is a concern during periods of particularly ambiguous image evidence, with samples likely to build up around an HMM state-mean. In anticipation we introduce a temperature parameter into the synthesis process, requiring a non-self state transition

from state i with some minimum probability ρ_T by making K_i state transitions. In general, hypotheses that extend too far along the activity cycle die out during annealing, discounted by comparison with image evidence in the evaluation of $w(\mathbf{z}_m, \mathbf{x}_m)$. However, where image evidence becomes weak, the approach is able to maintain a wider distribution of activity pose samples and escape becoming 'stuck' in an incorrect interpretation.

The remaining torso and head parameters are dispersed by the addition of Gaussian noise with diagonal covariance matrix \mathbf{P} estimated from the training data to give $\epsilon'_m | \epsilon'_{m-1}$. The covariance matrix is multiplied by the particle survival rate α^r at each annealing layer to give \mathbf{P}_r , the application of noise decreasing at the same rate as the resolution of the particle set increases [7]. We extend the scaling procedure to the observation densities at each HMM state $p_i(\mathbf{f}) = \mathcal{N}(\mathbf{f}|\boldsymbol{\mu}_i, \boldsymbol{\Sigma}_i)$ and to the transition temperature ρ_T , rescaling by α^r at each annealing layer to give $\boldsymbol{\Sigma}_i^r$ and ρ_T^r (or K_i^r transitions).

As the state means μ_i are constant, the effect of rescaling the observation densities during annealing is to force samples closer to the training data. For parameter reestimation in later annealing layers, self state transitions are more common as K_i^r becomes small. Where $s_j = s_i$ we uncouple the dispersion from μ_i and draw noise using a scaled version of the parent state's covariance matrix, Σ_i^r but replace μ_j with the particle's current estimate of $\mathbf{f}_m^{(b)}$. This stops the training data from dominating the choice of new pose hypotheses, allowing the weighting function scores to guide refinement. The particle dispersion process is summarised by the pseudocode listing in Figure 3.

3.3 Range Surface Weighting

The weighting function $w(\mathbf{z}_m, \mathbf{x}_m)$ provides an approximation of $p(\mathbf{z}_m | \mathbf{x}_m)$ by comparing the current observation and the geometric body model specified by $\mathbf{x}_m^{(b)}$. In standard APF [7], an evaluation of edge weighting is made by projecting the body model into the image and extracting a set of sample points $\{\xi\}$ from the edges of the component cones. The recovered coordinates are then used to compute a sum-squared difference (SSD) function,

$$-\log p(\mathbf{z}_m|\mathbf{x}_m) \propto \frac{1}{|\{\xi\}|} \sum_{\xi} (1 - V(\xi))^2, \tag{3}$$

where V is a smoothed edge image calculated from the current image data, \mathbf{z}_m . The edge image is calculated using a gradient based edge detection mask, smoothed by convolution with a 2D Gaussian kernel and rescaled to the range [0,1]. The result is a chamfer image where each pixel's value is proportional to its proximity to an edge.

We extend this approach to range data, discretising the (x,y,z) point cloud calculated by the stereo camera onto a 3D grid. The data describes 2.5D surfaces calculated from the disparity between the image pairs. We smooth the data by convolution with a 3D Gaussian kernel and rescale the values to the range [0,1]. The result is a chamfer volume where each voxel's value is proportional to its proximity to a surface. The chamfer volume is substituted for the chamfer image V in the calculation of the SSD. A hypothesis $\mathbf{x}_m^{(b)}$ is projected into the chamfer volume and sample points $\{\xi\}$ extracted from the visible surfaces of the body model's component cones are used in Eq. (3). Portions of the cones with surface normals pointing away from the stereo camera are omitted from the calculation as are sample points occluded by other nearer cones (denoted by empty circular markers in Figure 2(c)).

4 Experiments

4.1 Simulation

In order to investigate the effectiveness of parameters chosen for the training and tracking process we carried out a series of simulation experiments on synthetic walking trials. Test data from the same walking subject as the activity training data [5] was animated using a body model with dimensions estimated from their MoCap markers. The model's root position was held constant throughout to produce a pose recovery problem and we set torso location noise to zero in the estimation of \mathbf{P} . Range data relative to a fixed observation point was sampled from the visible surfaces of the cones at 30fps and used to create a set of chamfer volumes from which we attempted tracking. The particle set was initialised with ground truth and the weighted relative error computed at each frame using the average distance between the joint centres of each hypothesis and those of the true pose, weighted by $\pi_m^{(b)}$. Results using a range of state numbers to build the HMM and transition temperatures to traverse it are shown in Figure 4.

Each point plotted represents an average score from 10 separate tracks of the test sequence, with 4(b) also showing the best and worst tracking results. Figure 4(a) used a 75 frame sequence of straight-line walking to investigate the quality of pose recovery using different numbers of HMM states. Figures 4(b) and 4(c) used a 150 frame sequence featuring a more challenging change of direction. Using 40 particles, 5 annealing layers and $\alpha^R = \ldots = \alpha^1 = 0.5$ we found no significant improvement in performance using greater than 10 HMM states. Failures were observed when using only the HMM transition matrix A_{ij} (low ρ_T , Figure 4(b)) or Gaussian noise (SIR, Figure 4(c)) to track the longer sequence. Figure 4(c) shows the results of the proposed method with N=15 states and $\rho_T=0.6$ versus SIR performed in the latent space. The increase in SIR tracking error at around frame 60 is due to tracking failures during a relatively sharp turn in the test sequence. The proposed method maintains tracking throughout each of the 10 tests.

4.2 Range Tracking

We recorded a 5 second sequence of an unknown walking subject at 30fps using a Videre MDCS2-VAR stereo camera [1]. The camera was held by hand and continually adjusted to ensure the subject remained fully in shot. Range data was calculated using the commercially available Small Vision System software [1, 10] and discretised onto a 3D grid with a resolution of 4cm in each dimension before being smoothed with a $7 \times 7 \times 7$ Gaussian kernel. The torso location (not orientation) noise was halved in the estimation of \mathbf{P} to represent the fact that the camera follows the subject. The body model was hand-initialised and tracking attempted using 100 particles, 5 annealing layers, $\alpha^R = \ldots = \alpha^1 = 0.5$ and $\rho_T = 0.6$, results are shown in Figure 5 and demonstrate qualitatively satisfactory tracking of unknown subject walking from stereo range data.

5 Discussion and Future Work

The use of an activity model is consistent with recent approaches to monocular tracking [11, 15, 16, 17] and in future we intend to capture stereo data simultaneously with MoCap data for quantitative evaluation and comparison. We anticipate the method will give an

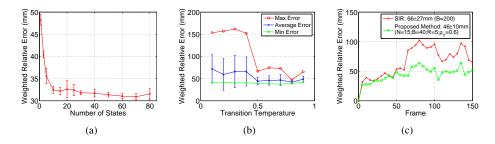


Figure 4: Simulation results. (a) Mean tracking error versus number of states; (b) Tracking error versus transition temperature ρ_T ; (c) SIR versus proposed method.

advantage over monocular approaches in terms of absolute tracking error as it is able to estimate the true 3D position of the subject relative to the sensor, rather than their pose alone. It should also perform well outdoors and in other more natural scenes where backgrounds are changing and lighting and shadows are not controlled.

As anticipated the depth cue is noisy and ambiguous but although some mis-tracking is seen, for example the right leg in Figure 5, tracking is each time recovered within a few frames. Although it is the use of an activity model that facilitates the recovery of errors, the constraints it places on the feature space also serve to restrict the ability to track new activity. Stylistic intra-activity differences between the training and test subjects are also visible, in the bend of the arms as they swing forward for example. The addition of more subjects to the activity training set might help to recover such variations but a more effective approach may be to further perturb the recovered particle set in a final annealing layer by applying low level noise in the original 31D feature space [13]. Projecting these candidates back into a space recovered by PCA at the next frame is computationally inexpensive in contrast to nonlinear alternatives such as the GPLVM. We aim to pursue the projection of particles into multiple pre-computed activity spaces for dispersal by distinct activity HMMs. In this way we hope to track and classify multiple activities, as samples concentrate in a particular activity space during the annealing process.

6 Conclusions

We have demonstrated a method for tracking known human activity from stereo data. The subject tracked is not featured in the training set and is filmed performing a relatively sharp turn against a cluttered background by a moving hand-held stereo camera. Although resulting range data are noisy, they are relatively insensitive to experimental conditions and the calculation of chamfer volumes offers a method for hypothesis evaluation using the recovered surfaces. We are able to achieve robust tracking by sampling candidates from a simulated activity axis defined by HMM states in a low dimensional latent space recovered from MoCap training data. Results suggest that a relatively noisy estimate of 2.5D surface data is a sufficient cue for human motion tracking where the activity class is known. The method can be easily applied to data captured using other range sensors, such as time-of-flight cameras.

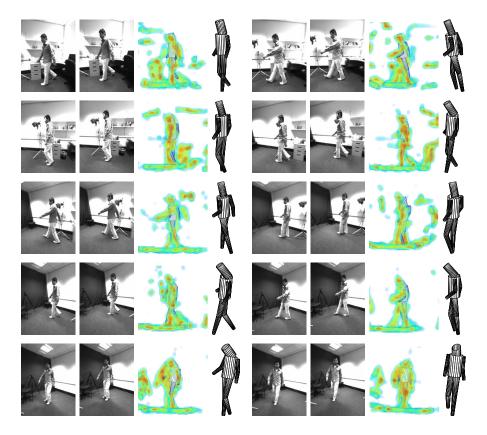


Figure 5: Stereo tracking results: B = 100 particles, R = 5 layers, every 15th frame.

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